LUMBAR SPINE COMPUTED TOMOGRAPHY AFTER ARTHRODESIS WITH METAL IMPLANT: A QUALITATIVE EVALUATION OF IMAGES RECONSTRUCTED WITH DIFFERENT MATHEMATICAL ALGORITHMS*

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Abstract OBJECTIVE: To select the best mathematical algorithms for lumbar spine imaging studies to assess arthrodesis with metal implant. MATERIALS E METHODS: The images acquisition was performed with a multidetector (16 rows) CT scanner, and 2 mm and 4 mm slice thickness. Images of ten patients were reconstructed with filters 20, 40, 60 and 80, employing multiplanar three-dimensional volume-rendering techniques. A total of 320 images were evaluated by three experienced radiologists who rated the images from 1 to 5 (1 = unacceptable; 2 = substandard; 3 = acceptable; 4 = above the average; 5 = excellent). Additionally, noise measurements were performed for correlation with the type of filter utilized. RESULTS: For 2 mm thickness and filters 20, 40, 60 e 80, mean noise measurements for images reconstruction were, respectively, 24.7 \pm 4.3, 35.5 \pm 4.2, 106.0 \pm 18.5 and 145.9 \pm 26.9, and for 4 mm and filters 20, 40, 60 and 80 were, respectively, 18.1 \pm 2.4, 25.1 \pm 4.6, 76.7 \pm 17.2 and 106.6 \pm 23.4. CONCLUSION: Three-dimensional color images could be better visualized with filter 20; however, in the case of gray-scale, filters 40 or 60 could be useful to demonstrate the arthrodesis pedicle screws in higher detail. For multiplanar reconstructions with 2 mm slice thickness, the filter 40 was the most appropriate, and for 4 mm, a filter 60 presented a better image quality.

Keywords: Computed tomography; Arthrodesis; Lumbar spine; Image quality.

Resumo Tomografia computadorizada da coluna lombar após artrodese com emprego de material metálico: avaliação da qualidade da imagem para diferentes algoritmos matemáticos.

OBJETIVO: Selecionar os melhores algoritmos para o exame de coluna lombar na avaliação de artrodese com material metálico. MATERIAIS E MÉTODOS: Utilizou-se um equipamento de tomografia computadorizada de 16 fileiras de detectores. Imagens de dez pacientes foram reconstruídas com filtros 20, 40, 60 e 80 e realizadas reformatações em três dimensões e multiplanares com espessuras de 2 mm e 4 mm. Um total de 320 imagens foi avaliado por três experientes radiologistas, que deram notas de 1 a 5 (1 = não-aceitável; 2 = abaixo dos padrões; 3 = aceitável; 4 = acima da média; 5 = excelente). Além disso, foram realizadas medidas de ruído para correlação com o tipo de filtro utilizado. RESULTADOS: As médias do valor de ruído para reconstrução com 2 mm e filtros 20, 40, 60 e 80 foram de 24,7 \pm 4,3; 35,5 \pm 4,2; 106,0 \pm 18,5 e 145,9 \pm 26,9, respectivamente, e para 4 mm foram de 18,1 \pm 2,4; 25,1 \pm 4,6; 76,7 \pm 17,2 e 106,6 \pm 23,4. CONCLUSÃO: As imagens coloridas em três dimensões são mais bem visualizadas com filtro 20, entretanto, nas imagens em tons de cinza um filtro intermediário de 40 ou 60 pode ser útil para demonstrar os parafusos com maior detalhe. Para reconstruções multiplanares com espessura de 2 mm o filtro 40 é mais bem aceito, e para uma espessura de 4 mm um filtro 60 apresentou melhor qualidade.

Unitermos: Tomografia computadorizada; Artrodese; Coluna lombar; Qualidade da imagem.

INTRODUCTION

Spinal fusion with metal implants has been utilized for some years, and postoperative evaluation may be performed by means of imaging diagnosis methods such us conventional x-ray, computed tomography (CT) or magnetic resonance imaging (MRI). These three methods present advantages and disadvantages, conventional xray being the lowest cost alternative although it does not allow a detailed visualization of the rachidian canal and soft tissues. In some cases, several views may be necessary. MRI is a less utilized method because of its high cost; additionally, metal implants may cause artifacts, which many times make the method unfeasible. On the other hand, multidetector CT is the most complete method, despite the disadvantage of its high cost when compared with the conventional x-ray⁽¹⁾.

As regards the radiation dose, an study of the United Nations Scientific Committee

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on the Effects of Atomic Radiation presents effective doses for conventional lumbar spine x-ray studies in several countries, ranging from low to high levels in relation to CT studies, depending on the parameters utilized as well as on the number of views⁽²⁾.

Currently, CT equipment can control the radiation dose according to the anatomical region and the size of the patient, resulting in a considerable reduction of the effective radiation dose. Additionally, such equipment present more advanced resources for the images reconstruction (multiplanar reconstruction - MPR), maximum intensity projection (MIP), and even high quality 3D images with the volume rendering technology (VRT). Also, there is the possibility of utilizing different mathematical algorithms, which are calculations performed by the tomograph computer in the moment of the images reconstruction, sharpening or softening them. These algorithms or filters have a direct influence on the images quality, changing both the spatial resolution and noise⁽³⁾.

Usually, in spine studies, a filter is utilized for visualizing bone, and other for visualizing soft tissues, on axial, sagittal and coronal views. However, for evaluating arthrodesis with metal implants, more detailed reconstructions, including 3D images, are necessary to reduce artifacts, and, for this purpose, the utilization of different filters is involved. The recently produced Siemens CT equipment has several filters specific for each region of the body, with values ranging between 10 and 90. The lower the filter value, the lower the noise and the better the low-contrast resolution on the images, which are ideal for visualizing soft tissues. When the filter value is increased, there is an increase in the noise and spatial resolution on the image, ideal for visualizing bone structures and highcontrast objects⁽³⁾.

The objective of the present study is to determine the most appropriate filters for lumbar spine CT evaluation after arthrodesis with metal implants.

MATERIALS AND METHODS

A multidetector (16 rows) CT equipment (Somatom Sensation Cardiac; Siemens AG) was utilized in the present study. Ten patients who had been submitted to CT of the lumbar-sacral spine for evaluation of arthrodesis with metal implant were selected. The examination was performed on a routine basis, under the following technical parameters: 120 kV, 200 mAs, reference and collimation 16 \times 1,5 mm. An automatic exposure control system (Care Dose; Siemens AG) was utilized. Post-processing with filters numbers 20, 40, 60 e 80 was requested. After that, 3D reformation was performed with VRT in gray-scale and color, MPR with 2 mm and 4 mm thickness, axial, sagittal and coronal, oblique views, with specific inclinators for better demonstrating pedicle screws, in a post-processing workstation (Wizard; Siemens AG). Three hundred and twenty images were presented without acquisition and reconstruction parameters for evaluation by three experienced Radiologists who subjectively rated them from 1 to 5 (1 = unacceptable; 2 = substandard; 3 =acceptable; 4 = above the average; 5 = excellent) as to spatial resolution, noise and artifacts. Reconstruction criteria were the same for the whole sample, the filter being the only variable factor. Therefore, each patient was his/her own control, and it was not necessary to select patents with similar characteristics, with the same type of metal implant or biotype. Measurements of noise level were performed on axial images for each type of filter and slices thickness, positioning a region of interest on the psoas muscle (Figure 1).

Statistical analysis

Grades and noise level measurements were included in a table and means and standard deviations were calculated. For determining the best types of filters for each type of reconstruction, a comparison between the averages of grades employing Friedman and Wilcoxon tests with Bonferroni correction. Interobserver concordance was analyzed with the kappa test.

RESULTS

Patients' data are shown on Table 1. The mean noise levels for reconstruction with 2 mm thick slices and filters 20, 40, 60 and 80 were respectively de 24.7 ± 4.3 , $35.5 \pm$



Figure 1. Axial image with the region of interest positioned on the psoas muscle for evaluation of the noise level.

4.2, 106.0 \pm 18.5 and 145.9 \pm 26.9; and with 4 mm thick slices were 18.1 \pm 2.4, 25.1 \pm 4.6, 76.7 \pm 17.2 and 106.6 \pm 23.4. The graphic on Figure 2 shows this variation for each type of filter.

Table 2 shows means and standard deviations of the grades given by the three observers.

The statistical analysis has proved the existence of a difference in the images for the several types of filters and slices thickness (p < 0.05). For the VRT reconstruction in grayscale (Figure 3), the filter 60 presented the best mean, although being statistically similar to that of the filter 60. On color VRT images (Figure 4), the best mean was that of filter 20. On the 2 mm thick sagittal reconstruction (Figure 5 – A,C, E,G), the highest mean was that of filter 20, although statistically similar to that for the

Table	1	Data	of	patients	included	in	the	study.
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	Weight	Number of metal elements			
Patient	(kg)	Screws	Rods		
1	75	6	2		
2	94	10	2		
3	60	8	2		
4	90	6	2		
5	60	4	2		
6	62	4	2		
7	60	4	2		
8	50	6	2		
9	62	4	2		
10	80	6	2		

	Filter 20		Filter 40		Filter 60		Filter 80	
Type of reconstruction	Mean	SD	Mean	SD	Mean	SD	Mean	SD
VRT gray scale	3.1	0.5	3.9	0.6	4.0	0.6	2.9	0.6
VRT color	4.3	0.5	3.8	0.7	1.6	0.4	1.4	0.4
Sagittal 2 mm	3.7	0.7	3.6	0.5	2.4	0.8	2.1	0.4
Sagittal 4 mm	3.5	0.4	3.8	0.4	4.3	0.5	3.4	0.6
Axial 2 mm	2.4	0.5	3.3	0.7	3.5	0.5	2.7	0.6
Axial 4 mm	2.3	0.5	3.2	0.6	3.7	0.4	2.5	0.4
Coronal 2 mm	3.1	0.4	3.3	0.6	2.3	0.5	1.8	0.3
Coronal 4 mm	3.1	0.3	3.5	0.4	4.2	0.5	3.2	0.9

filter 40. For the 2 mm thick (Figure 6 A,C,E,G) and 4 mm thick (Figure 6 – B,D,F,H) axial reconstructions with filter 60, the highest means has been obtained. For 2 mm thick (Figure 7 – A,C,E,G) and 4 mm (Figure 7 – B,D,F,H) coronal images, the highest means were, respectively, those of filters 40 and 60.

With basis on the statistical analyses, interobserver concordance was observed in relation to the sagittal and coronal 2 mm VRT reconstructions in color (p < 0.05). For the other reconstructions, the concordance was low.



Figure 2. Graphic showing the noise level variations for each type of filter with different slice thicknesses.

DISCUSSION

The postoperative evaluation is aimed at assuring the diagnosis of the dural sac and nervous roots integrity; observing alignment and bone fixation, the metal material mechanics and integration; verifying the previous disease correction degree; and identifying eventual complications like hematomas, inflammatory processes, etc.

The utilization of an appropriate technique in the images reconstruction is ex-



Figure 3. VRT reconstructions in grayscale. A: Filter 20; B: filter 40; C: filter 60; D: filter 80.



Figure 4. VRT reconstructions in color. A: Filter 20; B: filter 40; C: filter 60; D: filter 80.





Figure 5. Sagittal oblique reconstructions. A: Filter 20 with 2mm de slice thickness; B: filter 20 with 4mm de slice thickness; C: filter 40 with 2mm de slice thickness; D: filter 40 with 4mm de slice thickness; E: filter 60 with 2mm de slice thickness; F: filter 60 with 4mm de slice thickness; G: filter 80 with 2 mm de slice thickness; H: filter 80 with 4mm slice thickness.

tremely important, mainly in studies susceptible to artifacts. In such cases, a complete elimination of artifacts is practically impossible, however, they can be reduced to an acceptable level to not impairing the diagnosis. The CT in the evaluation of arthrodesis has been always very problematic⁽⁴⁾ because of beam hardening artifacts, but the introduction of the multidetector or multislice CT has brought a new perspective for these studies. The quality of the volume rendering and images reconstruction resources has improved considerably in relation to the previous technologies⁽⁵⁾.

In the images acquisition process, the noise level is directly related to the radiation dose, the collimation of detectors, and the slice reconstruction thickness; on the other hand, the spatial resolution is influenced only by the collimation of detectors. In the reconstruction phase, filters or mathematical algorithms should be considered in addition to slice thickness, since the equipments allow an array of combinations between filters and slice thicknesses.

Based on the results of the present study, we could observe that lower filter values



Figure 6. Axial, oblique reconstructions. A: Filter 20 with 2mm de slice thickness; B: filter 20 with 4mm de slice thickness; C: filter 40 with 2mm de slice thickness; D: filter 40 with 4mm de slice thickness; E: filter 60 with 2mm de slice thickness; F: filter 60 with 4mm de slice thickness; G: filter 80 with 2mm de slice thickness; H: filter 80 with 4 mm de slice thickness.



Figure 7. Coronal, oblique reconstructions. A: Filter 20 with 2mm slice thickness; B: Filter 20 with 4mm slice thickness; C: filter 40 with 2mm slice thickness; D: filter 40 with 4mm slice thickness; E: filter 60 with 2mm slice thickness; F: filter 60 with 4mm slice thickness; G: filter 80 with 2 mm slice thickness; H: filter 80 with 4mm slice thickness.

and greater slice thicknesses result in a decrease in the spatial resolution and noise reduction of the reconstructed images. A low noise level is highly favorable to color 3D reconstructions with the VRT technique, resulting in high quality images of the lumbar spine. In the analysis of grayscale images obtained with VRT which present a certain transparency allowing the demonstration of the pedicle screws, the Radiologists gave higher grades for reconstructions with intermediate filters like 40 and 60. These results are justified by the higher spatial resolution allowing a better visualization of grooves or alterations on pedicle screws. In the analysis of MPR images, filter 20 and 80 received the lowest grades. The use of filter 20 results in a very low definition of borders and bone trabeculations due the lower spatial resolution. The filter 80, on the contrary, accentuates borders and noises. On the other hand, filters 40 and 60 had a better performance with slice thicknesses of 4 mm and 2 mm, respectively. As previously mentioned, with lower slice thicknesses, there is an increase in spatial resolution and noise level, so the increase in noise level, as a result of a 2 mm slice thickness, is balanced by the filter 40, and the decrease in spatial resolution resulting from 4 mm slice thickness is balanced by the filter 60.

Images were subjectively analyzed by the radiologists who have given higher grades to images gathering the most comprehensive set of positive factors like a balance among spatial resolution, noise level and artifacts. In the daily practice, the protocol for images acquisition and reconstruction must be adequately standardized to attain similar results in terms of images quality for every patient. The utilization of several combinations of filters and slice thicknesses is not recommended because of its impracticability, besides the high number of images generated. Therefore, a type of filter for color VRT images, and another for MPR are sufficient.

The noise level increased gradually as the filters were changed from 20 to 80. Also, the 2 mm slice thickness showed a higher noise level in relation to the 4 mm slice thickness. On the whole, color 3D-VRT images are better visualized with filter 20 because of the lower noise level, however, on grayscale VRT images, an intermediary filter 40 or 60 might be of help to demonstrate pedicle screws in higher detail. In spite of the disagreement of the physicians' opinions on MPR images, the conclusion is that, for a 2mm slice thickness the filter 40 is the best for balancing the noise resulting from the slice thinness, and with a 4 mm slice thickness, a filter 60 results in a better quality of image.

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REFERENCES

- Williams AL, Gornet MF, Burkus JK. CT evaluation of lumbar interbody fusion: current concepts. AJNR Am J Neurorradiol 2005;26:2057– 2066.
- United Nations Scientific Committee on the Effects of Atomic Radiation. UNSCEAR 2000 Report to the General Assembly, with scientific annexes. Annex D. New York: United Nations, 2000.
- Seeram E. Computed tomography. Physical principles, clinical applications, and quality control. 2nd ed. Philadelphia: WB Saunders, 2001.
- 4. Cook SD, Patron LP, Christa Kis PM, et al. Comparison of methods for determining the presence

and extend of anterior lumbar interbody fusion. Spine 2004;29:1118–1123.

 Cody DD, Moxley DM, Davros W, Silverman PM. Principles of multislice computed tomography technology. In: Silverman PM, editor. Multislice computed tomography. A practical approach to clinical protocols. 1st ed. Philadelphia: Lippincott Williams & Wilkins, 2002;1–29.